# DEVELOPMENT OF ELECTROCHEMICAL BIOSENSOR BASED ON SnO<sub>2</sub>-NANOFIBER WITH ENHANCED ELECTRON TRANSFER OF REDOX BIOMOLECULE

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We hereby declare that we have checked this thesis and in our opinion, this thesis is adequate in terms of scope and quality for the award of the degree of Master of Science.

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I hereby declare that the work in this thesis is based on my original work except for quotations and citations which have been duly acknowledged. I also declare that it has not been previously or concurrently submitted for any other degree at University Malaysia Pahang or any other institutions.

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SAMIUL ALIM

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#### ABSTRAK

Biosensor jenis elektrokimia sangat sesuai untuk pemantauan kandungan  $H_2O_2$ , glukosa, kolesterol, petanda barah, penyakit berjangkit berkaitan, dan sebagainya. Tetapi pembangunan biosensor elektrokimia dengan enzim pautan mengalami cabaran besar seperti kekurangan gandingan elektronik yang baik dan hubungan elektrik di antara tapak aktif protein / enzim redoks yang digunakan dan permukaan elektrod. Oleh itu sebagai satu jalan penyelesaian, banyak usaha telah nanofiber (NF) SnO<sub>2</sub> sebagai bahan nano terunggul dalam biosensor. Usaha utama disertasi ini adalah untuk menguji peranan kritikal yang dimainkan oleh bahan nano tersebut apabila ia digunakan dalam pembangunan biosensor elektrokimia dengan cara immobililasikan protein redoks atau enzim yang berbeza. SnO<sub>2</sub>-NF yang digunakan dalam penyelidikan ini disintesis dengan cara teknik elektrospinning dari prekursor timah. Campuran SnO<sub>2</sub>-NF yang disintesis meningkatkan kecekapan muatan biomolekul kerana kawasan permukaan yang tinggi tercapai. Morfologi nanofiber yang disintesis juga telah dinilai oleh mikroskop elektron pengimbasan emisi lapangan (FESEM) dan spektrometer sinaran sinar-X (EDX). Sebelum ini, biosensor H<sub>2</sub>O<sub>2</sub> amperometri telah direka berdasarkan enzim "horseradish peroxidase" (HRP) dengan NF SnO2 diletak pada permukaan elektrod karbon gelas (GC) dengan menggunakan "chitosan", yang didapati bertindak balas cepat iaitu dengan had pengesanan yang lebih rendah iaitu 0.3 µM (S/N=3). Biosensor HRP/SnO<sub>2</sub>-NFs/Ch/GCE yang direka menunjukan lineariti antara kepekatan 10 hingga 120 µM H<sub>2</sub>O<sub>2</sub>. Untuk menilai prestasi nanofiber SnO<sub>2</sub> yang diubahsuai dalam biosensor, biosensor H<sub>2</sub>O<sub>2</sub> berasaskan HRP kemudian pula direka, yang mana NF dengan SnO<sub>2</sub> telah di polimerisasi dengan polyaniline (PANI) dan enzim HRP telah dimobilisasi dengan PANI/SnO2 ini ke permukaan GC. Biosensor HRP/PANI/SnO2-NF/Ch/GC ini yang direka membuat tindak balas amperometri linear ke arah kepekatan H<sub>2</sub>O<sub>2</sub> dari julat 10 hingga 80 µM dengan nilai had pengesanan 0.133 µM (S/N=3). Biosensor pengesanan glukosa dengan guna enzim kemudian direka dan rekaan berdasarkan SnO<sub>2</sub>-NF dengan polimer bersama glukosa oksidase (GOx) dan horseradish peroxidase (HRP) dengan ini dengan menggunakan chitosan ke elektrod karbon kaca. Biosensor ini direka untuk menilai potensi keupayaan SnO<sub>2</sub>-NFs dalam pembangunan biosensor dengan dua jenis bi-enzim. Biosensor HRP-GOx/PANI/SnO<sub>2</sub>-NF/Ch/GCE memaparkan tindak balas amperometri linear ke arah kepekatan glukosa antara 10 hingga 110 µM dengan had pengesanan sebanyak 1.8 µM (S/N=3). Aktiviti anti-perencatan juga disiasat. Akhirnya, SnO<sub>2</sub>-NF dengan tiub nano karbon (CNTs) dan chitosan digunakan bersama untuk fabrikasi biosensor H<sub>2</sub>O<sub>2</sub> terunggul lain untuk menilai kesan sinergi SnO<sub>2</sub>-NFs dengan bahan nano lain dalam biosensing. Protein redoks (Hemoglobin) telah dimobilisasi dengan nanocomposite CNT/SnO<sub>2</sub>-NF dengan menggunakan chitosan di permukaan GC. Elektrod Hb/CNT/SnO<sub>2</sub>-NF/Ch/GC yang dihasilkan efektif kepada kepekatan  $H_2O_2$  dalam pelbagai antara 10 hingga 200  $\mu$ M dan had pengesanan paling rendah ialah 30 nM (S/N=3). Didapati pemindahan elektron langsung antara pusat aktif protein/enzim redoks dan permukaan elektrod telah terhasil dengan jayanya kerana menggunakan nanofiber ini dan semua biosensor yang dilaporkan dalam kerja ini mempamerkan keupayaan selektiviti yang sangat baik juga kestabilan, dan kebolehulangan.

#### ABSTRACT

Electrochemical biosensors are highly desirable for the monitoring of H<sub>2</sub>O<sub>2</sub>, glucose, cholesterol, cancer biomarkers, infectious diseases, etc. But the development of enzymatic electrochemical biosensors is oppressed with great challenges like the lack of good electronic coupling and electrical contact between the active site of the used redox protein/enzyme and the electrode surface. Hence, a great deal of effort has been devoted by using nanofiber (NF) of SnO<sub>2</sub> as nanomaterial in biosensor to deal with this challenge. Thus, the main theme of this dissertation pertains to highlighting the critical roles that are played by this nanomaterial when this is applied in the development of electrochemical biosensors by immobilizing different redox proteins or enzymes. The SnO<sub>2</sub>-NFs used in this research was synthesised by electrospinning technique from the tin precursor. The synthesized SnO<sub>2</sub>-NF increases the efficiency of biomolecule loading due to its high surface area. The morphology of the nanofiber was evaluated by field emission scanning electron microscopy (FESEM) and energy-dispersive X-ray (EDX) spectrometer was used for evaluating the sterility of the synthesized nanofiber. For this research project, an amperometric H<sub>2</sub>O<sub>2</sub> biosensor was designed and fabricated firstly based on the immobilization of horseradish peroxidase (HRP) enzyme with NF of SnO<sub>2</sub> onto the surface of glassy carbon electrode (GC) by using chitosan, which exhibited fast response with lower detection limit of 0.3 µM (S/N=3). The fabricated HRP/SnO<sub>2</sub>-NF/Ch/GC biosensor showed linearity ranges between the concentration of 10 to 120  $\mu$ M H<sub>2</sub>O<sub>2</sub>. To evaluate the performance of the modified SnO<sub>2</sub> nanofiber in biosensor, a HRP based H<sub>2</sub>O<sub>2</sub> biosensor was then designed and fabricated, whereas, the NFs of SnO<sub>2</sub> was polymerized with polyaniline (PANI) and HRP enzyme was immobilized with this PANI/SnO2 onto the surface of GC. The fabricated HRP/PANI/SnO2-NF/Ch/GCE biosensor displayed a linear amperometric response towards the H<sub>2</sub>O<sub>2</sub> concentration range from 10 to 80 µM with a detection limit of 0.133 µM (S/N=3). A bienzymatic glucose biosensor was then designed and fabricated based on the polymerized SnO<sub>2</sub>-NF via co-immobilization of glucose oxidase (GOx) and horseradish peroxidase (HRP) with this by using chitosan onto glassy carbon electrode. This biosensor was fabricated to evaluate the potentiality of SnO<sub>2</sub>-NF in the development of bienzymatic biosensor. The HRP-GOx/PANI/SnO<sub>2</sub>-NF/Ch/GC biosensor displayed a linear amperometric response towards the glucose concentration range from 10 to 110 µM with a detection limit of 1.8  $\mu$ M (S/N = 3). Also the anti-interference activity was investigated. Finally, SnO<sub>2</sub>-NF with Carbon nanotubes (CNT) and chitosan was used together for the fabrication of another novel H<sub>2</sub>O<sub>2</sub> biosensor to evaluate the synergic effect of SnO<sub>2</sub>-NF with other nanomaterial in biosensing. A redox protein (Hemoglobin) was immobilized with CNT/SnO<sub>2</sub>-NF nanocomposite by using chitosan on the surface of GC. The fabricated Hb/CNT/SnO<sub>2</sub>-NF/Ch/GC electrode exhibited linearity to the H<sub>2</sub>O<sub>2</sub> concentration in a wide range of 10 to 200 µM and the lower detection limit was 30 nM (S/N=3). A direct electron transfer between the active center of redox protein/enzyme and the electrode surface was established because of using this nanofiber and all the biosensors reported in this work exhibited excellent selectivity with stability, reproducibility and repeatability.

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# LIST OF SYMBOLS

A	Geometric area of the working electrode
С	Concentration
$E_0$	Formal potential
$E_{pa}$	Anodic peak potential
$E_{pc}$	Cathodic peak potential
I	Current
I <sub>max</sub>	Maximum current
$I_p$	Peak current
Iss	Steady state current
K <sub>m</sub> ,	Michaelis-Menten constant
ks	Interfacial electron transfer rate constants
n	Number of transferred electrons
v	Scan rate
S	Signal
Ν	Noise

# LIST OF ABBREVIATIONS

LOD	Limit of Detection
RSD	Relative standar deviation
FESEM	Field Emission Scanning Electron Microscopy
CV	Cyclic Voltammetry
SEM	Scanning Electron Microscopy
HRP	Horseradish peroxidase
GOx	Glucose oxidase
EDX	Energy-dispersive X-ray spectroscopy

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