

Neuro-modelling and fuzzy logic control of a two-wheeled wheelchair system

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NIzaruddin M. Nasir¹, Nor Maniha Abdul Ghani¹⁰, Ahmad Nor Kasruddin Nasir¹, Mohd Ashraf Ahmad¹ and Mohammad Osman Tokhi²

Abstract

Two-wheeled wheelchairs have been used as alternatives for the elderly and disabled people to perform physical activities due to their restriction of movement. Significant challenges posed by two-wheeled wheelchairs control due to their inherent instability, resembling that inverted pendulum system. This research addresses these challenges by developing a dynamic non-linear model and stability control using computational algorithms. A neural network-based Nonlinear Autoregressive model with Exogenous Inputs (NARX) was developed, capturing and behaving similar to the complex dynamics of the wheelchair system with the identification on the experimental input–output data. Ensuring stable and responsive control, design of optimized PD-type and PID-type fuzzy logic controllers using Particle Swarm Optimization (PSO) were established and were tested under a simulation environment. The performance was evaluated across various metrics, including Integral Squared Error (ISE), Integral Absolute Error (IAE), Mean Squared (MSE), and Integral Time Absolute Error (ITAE). The result demonstrates that the PSO Optimized PID-type fuzzy logic controller with scaling factor from MSE index performance come out as best overall, significantly outperforms PD-type fuzzy logic controller, reducing its settling time by 12.5% to 35 s, minimizing overshoot to 0.81°, and achieving a negligible steady-state error of 0.046%. These results highlight the significant of integrating fuzzy logic control and PSO to the neural network model in enhancing the stability and performance of two-wheeled wheelchair systems, offering user safety and comfort.

Keywords

Neural network, fuzzy logic control, particle swarm optimization, system identification, two-wheeled wheelchair

Introduction

A wheelchair is an effective instrument for elderly and disabled people since it will provide them with autonomy in their daily mobility tasks. There are 35.2% of disabled people in Malaysia who are physically handicapped.¹ It is well-recognized that a wheelchair is a significant way for the elderly and handicapped to travel from place to place.² Normally, a four-wheeled wheelchair configuration is used for disabled people, however, the standard four-wheeled wheelchairs have some limitations in their design, namely, they are bulky, the user cannot reach higher heights and are difficult to maneuver in narrow/confined spaces. By using a two-wheeled wheelchair, the users can reach a higher level of height, confidently perform eye-to-eye level of conversation with normal people,³ and maneuver easily in confined spaces.

A two-wheeled wheelchair mimics an inverted pendulum system, known to be a complex, unstable, and highly nonlinear system. Thus, the stability of a two-wheeled wheelchair poses control challenge, and it becomes more complicated during maneuvering and has the same dynamics as a self-balancing inverted pendulum system, which is known as a precarious system.^{4–9} Its popularity follows the fact that it is unstable without control, the upper part of the inverted

Corresponding author: Nor Maniha Abdul Ghani, Faculty of Electrical and Electronics Engineering Technology, Universiti Malaysia Pahang Al-Sultan Abdullah, Pekan Campus, Pekan, Pahang 26600, Malaysia. Email: normaniha@umpsa.edu.my



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¹Faculty of Electrical & Electronics Engineering Technology, Universiti Malaysia Pahang Al-Sultan Abdullah, Pekan Pahang, Malaysia ²School of Engineering, London South Bank University, London, UK

pendulum will fall over if the lower part is not moved to balance it. The goal of controlling this system is to balance the pendulum by applying a force to the lower part, for instance, the cart. Extensive research on balancing the inverted pendulum has been conducted due to its importance in the control engineering field.¹⁰ Few control approaches have been developed to stabilize a two-wheel inverted double-link pendulum mechanism. These include fuzzy logic-based control,^{11–13} Neural network-based control,^{14,15} swing-up scheme control,¹⁶ and hybrid LQR-fuzzy control.^{17,18} Moreover, these approaches have involved the cascading of Proportional Integral Derivative (PID) control,^{19–21} group of Sliding Mode Control (SMC),^{22,23} and Proportional Derivative (PD) control.²⁴ Changes can be made on the inverted pendulum system, for instance, the increment of links system for an additional degree of freedom, and different types of actuators to move the system; these changes will increase the complexity of the system. For example, there are single link inverted pendulum,²⁵ double link inverted pendulum,⁴ and triple link inverted pendulum,²⁶ while their actuator could be on a cart,²⁵ on two wheels,²⁶ on a rotary wheel or inertia wheel. In general, all these systems share the same characteristic; they are inherently unstable. Although there are various successful cases on controlling the inverted pendulum by using conventional controllers such as PID and Linear Quadratic Regulator (LQR), however, most of these have been developed and evaluated only in simulation studies.^{26–30}

The complexity and uncertainties of an actual system in real scenarios become a significant issue in maintaining system stability to ensure user's comfort and safety through reduction of overshoot and steady state error minimization. From previous literature studies, it is found that the two-wheeled wheelchair system lacks in utilizing an intelligent approach to model and control the stability of the tilt angle in real hardware platform. Therefore, intelligent controller-based optimization algorithm is proposed to overcome the close-loop unstable problem and stabilize the two-wheeled wheelchair in an upright position specifically in real two-wheeled wheelchair hardware system model and control testing scenarios.

Recently, optimization techniques-based Particle Swarm (PSO) algorithm is adopted to determine optimum control performances specifically for stability of inverted pendulum system.^{31,32} Particle Swarm Optimization is an evolutionary computation method inspired by the swarming or collaborative behavior of biological populations. PSO is initialized with a collection of random particles or solutions and then the generations are altered to check for optimum. In iteration, the two "best" values are used to update each particle. Moreover, in this work, the designed controller is also optimized using well and established PSO algorithm to achieve optimum result due to these two best values compared to other optimization algorithms.

System identification has been introduced to overcome the limitation of knowledge on system dynamics, it leverages the experimental data of system to obtain an authentic dynamic model during testing and characterizing the system behaviors. System identification on a two-wheel self-balanced mobile robot is conducted by collecting the input-output data from open-loop system and carry out.³³ It conducted system identification with linear models such as Autoregressive with Exogenous Input (ARX), Autoregressive Moving Average Model (ARMAX), Box Jenkin (BJ), and Output Error (OE), as well as nonlinear models like Wiener and Hammerstein. The nonlinear models able to describe the nonlinearity of a dynamic system effectively and Wiener type model structure is the best model to modelling highly nonlinear system with acceptable accuracy. Previous literature discusses the system identification of a MISO two-wheel inverted pendulum mobile robot. It starts from collecting input–output data from closed-loop system which have LQR controller as stabilization control. Then, system identification with models such as ARX, ARMAX, BJ, and OE are carried out, and results showed that ARX model is the best in representing the two-wheel inverted pendulum mobile robot.³⁴

The main contribution of this work is the development of an optimized controller based on PSO for the two-wheeled wheelchair system model obtained from real hardware. The dynamic behavior of the system is modelled using input-output data acquired directly from the experimental rig. A system identification based on neural network approach is adopted to model the system as the system exhibits highly non-linear behavior. This neuro-modelling technique and optimized controller specifically for two-wheeled wheelchair problem has not been found in any previous literature study.

System identification and neuro-modeling of two-wheeled wheelchair hardware

A system identification method is adopted here for obtaining a dynamic model of the two-wheeled wheelchair. The input and output system data are collected and utilized for training, testing, and validation purposes. The experimental data were collected from the two-wheeled wheelchair for development of the system model for use through this research. The input and output data of the two-wheeled wheelchair were the motor speed and angular position of wheelchair, respectively. These data were fetched into a non-linear autoregressive model with exogenous Inputs (NARX) Neural Network (NN) constructed in MATLAB for the system identification process. This step was crucial as the model generated represented the actual system dynamics. The data fetched were trained and tested for different NN configurations to obtain an accurate system model with the lowest mean-squared error (MSE). Fuzzy logic controllers (FLCs) were then developed for balancing the wheelchair in the upright position. In this study, two FLCs (PD-type fuzzy logic and PID-type fuzzy logic) were developed and designed with normalized membership function and compensated with a scaling factor to scale the membership function range. Finally, as the controllers are built with normalized membership function, gains will be needed to scale the membership function to suit the needs of stabilization control. Therefore, particle swarm optimization (PSO) was utilized to obtain the optimal gains for the controller. During this process, four different fitness functions, namely, Integral Squared Error (ISE), Integral Absolute Error (IAE), Integral Time Absolute Error (ITAE), and Mean Squared Error (MSE) were tested to determine the optimal scaling gains. Figure 1 shows a block diagram representation of the control structure.

The reference input is set to 0° to maintain the two-wheeled wheelchair in an upright position. An error signal is determined with the difference of reference angle and the actual angular position of the system. FLC is implemented to control the actuator input for the system to have an appropriate response. Since the scaling of membership function in FLC is obscure, PSO is added to aid the tuning of membership function scaling. The two-wheeled wheelchair used to produce the plant model was fabricated beforehand, and it is capable of accommodating humans. The specifications of the two-wheeled wheelchair are presented in Table 1.

Firstly, system identification was carried out with a closed-loop system. Since the two-wheeled wheelchair was openloop unstable, a stabilization controller implemented so to increase system run time and that the experimentally collected data will show the system dynamics. Figure 2 shows the components that were used to collect the input–output data.

Data collection method was used as in Figure 2,³⁵ with the motor speed as the input of two-wheeled wheelchair and the angular position as the output data. The input and output data were procured to the neural network for system identification. Firstly, the two-wheeled wheelchair was lifted and maintained in an upright position manually. Then the gyroscope was activated, and the calibration of its angular position automatically began. The calibration will take a few seconds to complete, and the two-wheeled wheelchair will stabilize itself. Although the PID controller was not able to stabilize the system it attempted to prevent the wheelchair from falling off instantly, which is vital for the system dynamics collection. The system was then left to run for a few minutes to collect the system's dynamics in the form of motor speed and angular position. A chain set was connected from a hoist to the two-wheeled wheelchair body, as a safety precaution, to ensure that the wheelchair will not fall off but loose enough to let the wheelchair move freely. The input–output data thus collected is presented in Figure 3.

The input and output data were captured and displayed via a serial monitor in Arduino IDE as in Figure 3. The input data, the motor speed and the output data, angular position was captured in the same interval of time. The gyroscope sensor was used to send the angular position of the wheelchair to the microcontroller, whereas the input data were the controlled effort of the PID controller. The motor speed data was measured in revolution per second (RPS) and the angular position was measured in degree. These datasets then will be used to train the neuro-model to develop similar to simulation of two-wheel wheelchair.



Figure 1. Block diagram of the control structure.

	Table I	۱.	Two-wheeled	d wheel	chair	specif	ication.
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Parameters	Value	Unit
Wheelchair	Two-wheeled	_
Weight	80	Kg
Length	0.645	m
Width	0.826	m
Height	1.4	m



Figure 2. Components of two-wheeled wheelchair.



Figure 3. The collected input-output data.

In this work, the neuro-modelling employs a perceptron-based artificial neural network (ANN) with embedded neuronbased function and is referred to as the perceptron of the neuro model. A linear combiner calculates the product of input vector, x of the neuron and the parameter vector, whereas a non-linear activation function is subjected to the output of the linear combiner.

Since the two-wheeled wheelchair is highly non-linear, NARX model was chosen as the model framework due to its simplicity. For estimating the non-linear part of the ARX structure, the NN is utilized, which has the ability to learn a set of data.^{36,37} It includes nodes organized into two or more separate layers.^{38,39} NNs are mathematically designed to mimic the biological neurons in the brain. They have been used extensively for identification of nonlinear dynamic systems.

A NARX neural network is set up by using the MATLAB neural network toolbox. The configuration of the network is realized with plant input-output data, hidden neurons, and number of delay signals. The training parameters, such as the number of neurons and the number of delay signals, are adjusted to obtain the best model. The NARX NN was created with 10 neurons in the hidden layer and 2 delay signals.

A total of 5773 datasets were used for the neural network training, testing, and validation. The data was distributed into three blocks where the training data consisted of 70% of the dataset, and the testing and validating data constituted 15% each. The validation step was crucial to determine the accuracy of the model estimated in resembling an actual two-wheeled wheelchair. After the network was trained, it underwent testing and validating process, and the final MSE was used to determine the best model. A heuristic method was used for the NN construction since there was no prior information about the appropriate number of delay signals and model structure. There were three main factors for consideration during the process: delay signals, the number of neurons in the hidden layer, and the error. The third factor was assessed along with the process of getting the best number of delay signals and the structure for each model.⁴⁰

Fuzzy logic control (FLC) systems imitate the human decision-making process based on rules to solve complicated nonlinear control problems. Most human knowledge is imprecise, uncertain, and usually expressed in linguistic terms. In addition, human ways of reasoning are approximate, and non-quantitative in nature. Fuzzy logic is a tool for transforming such linguistically expressed knowledge into a workable algorithm.

Using the corresponding membership functions, the output of a fuzzy controller is generated from a combination of both fuzzified inputs and outputs. A crisp input is translated based on its value into various members of the corresponding membership functions. From this viewpoint, a fuzzy logic controller's output is dependent on its membership of the various membership functions, which can be viewed as a set of inputs.

Both the FLCs are built using the MATLAB Fuzzy Logic toolbox. This toolbox simplifies the development of controller by changing the parameters in the GUI. Membership function and fuzzy rules can be altered in the toolbox easily, and the produced controller can be seamlessly used in MATLAB Simulink. All the membership functions are generalized in the range of -1 to 1 so that they create a scaling factor for optimization to take place. The following subsections elaborate on two types of FLC used in this study.

PD-FLC and **PID-FLC**

PD-FLC

Mandani type fuzzy logic was utilized in the design of PD-type FLC and the design of this controller is based on Ref.⁴¹ All the input and output crisp data were sent into the FLC, and they were put through Gaussian membership. Gaussian membership was chosen to accommodate the fuzzy logic set because it was more flexible and easier to represent and optimize. Table 2 shows the fuzzy rules used to set up the PD-type FLC.

PID-FLC

This controller is designed to adhere to the PID-type FLC design using Sugeno type fuzzy logic.⁴² All the input crisp data are sent into the fuzzy logic controller, and they go through triangular membership while the output data go through a constant membership function.

Simulink setup

The goal for this study is to maintain a two-wheeled wheelchair in the upright position and this is realized with the neuromodel and FLC described in the previous section. Figure 4 shows the block diagram of the closed-loop two-wheeled wheelchair system with PD-type and PID-type controllers.

PD-type FLC has two scaling factors for controller inputs and one scaling factor for controller output. On the other hand, PID-type controller has two scaling factors for controller input and two scaling factors for controller output.

PSO algorithm

An optimization algorithm is used in this work for efficient determination of optimal scaling factors of the FLC, as a trialand-error approach is time-consuming and nearly impossible for such a task. PSO is chosen in this study to carry out the

E\dE	NB	NS	Z	PS	PB
NB	PB	PB	PB	PS	Z
NS	PB	PB	PS	Z	NS
Z	PB	PS	Z	NS	NB
PS	PS	Z	NS	NB	NB
PB	Z	NS	NB	NB	NB

 Table 2.
 Rule base for PD-type FLC.



Clock To Workspac

(a) PD-type FLC



Figure 4. The simulink block diagrams of the FLCs (a) PD-type FLC (b) PID-type FLC.

optimization process. PSO is an evolutionary computation method inspired by the swarming or collaborative behavior of biological species.^{43,44} PSO is initialized with a collection of random particles (potential solutions), and they evolved and checked for their fitness through several iterations until convergence to an acceptable set is achieved. The PSO algorithm is based on the following two equations: -

$$v_{id} = v_{id} + c_1 rand()(p_{id} - x_{id}) + c_2 Rand()(p_{gd} - x_{id})$$

$$x_{id} = x_{id} + v_{id}$$
(1)

where v_{id} and x_{id} represent to velocity (trajectory) and position of particle *i* in the search space of dimension *d*. c_1 (cognition factor) and c_2 (social factor) represent the acceleration coefficients or learning factors. p_{id} (local guide) and p_{gd} (global

(abast), respectively, rand() and Rand() are random number

guide) represent the particle best (*pbest*) and global best (*gbest*), respectively, rand() and Rand() are random numbers in the range [0, 1]. The *pbest* and *gbest* are monitored at each iteration and compared to those achieved in previous iteration, if the values are better, they will replace the previous values and vice versa. This process continues until the stopping criterion is met, that is, either certain error minimum achieved, or maximum set number of iterations completed.

Table 3 shows the PSO parameters that were used for the optimization process. These parameter values were obtained from heuristic trial and error approach to give optimum performance of PSO algorithm. It was found that the performance of optimization is significantly affected by the number of particles and the number of iterations after several heuristic attempts. Table 4 shows the ranges of the scaling factors for controllers.

Various performance indexes such as *ISE*, *IAE*, *ITAE*, and *MSE* are accessed with the optimization of PD-PI controller for the control of the inverted pendulum.⁴⁵ Modern complex control systems usually oblige performance requirements that are more complicated than those provided so far. Error and time are critical factors that must be considered at the same time. A performance index is a single measure of the performance of a system that highlights the response characteristics that are considered important. In an estimator design using linear-state variable feedback, the notion of a performance index is very important.

The *ISE*, *IAE*, *ITAE* and *MSE* are determined, and they are used in the optimization of the controller for two-wheeled wheelchair stabilization. These are implemented for individual controller optimization as given below. Here, *t* represent the time and e(t) represents the error at time *t*.

$$IAE = \int_{0}^{\infty} |e(t)| dt$$
(2)

$$ISE = \int_{0}^{\infty} e^{2}(t) dt$$
(3)

$$ITAE = \int_{0}^{\infty} t|e(t)|\,dt \tag{4}$$

Table 3. Settings for PSO algorithm.

PSO parameter	Value
Number of particles	100
Number of iterations	50
Learning factor 1	0.12
Learning factor 2	0.2
Minimum weight	0.4
Maximum weight	0.9

	Table 4.	Range of	scaling	factors for	[•] PD-type	and PID-ty	pe FLC.
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FLC	Scaling factor	Gain
PD-type	KI	[0.001 1]
<i>/</i> /	К2	[0.001 0.1]
	К3	[000]
PID-type	KI	[0.001 1]
	К2	[0.001 0.1]
	К3	[0001]
	К4	[1 1000]

$$MSE = \int_{0}^{\infty} te^{2}(t) dt$$
(5)

Results: hardware testing and model validation

The identification process was initially carried out by changing the number of delay signals to predict the one-step-ahead (OSA) reaction. OSA is coherent with the dynamical structure of the system modelling as forecasting, involving with future state of the system referring on the current and past inputs. Accuracy of each prediction is paramount to ensure stability and performance of the control system.

To evaluate and fine-tune the predictive accuracy of this model, MSE indexes was chosen as the primary indicator. MSE quantifies the average of the squared differences between the predicted and actual values which appropriate with OSA predictions. Specifically emphasizing larger errors helps in identifying and minimize the deviation of those predictions. The sensitivity characteristics of MSE ensure not just an accurate model on average but also provide robust features in scenarios where it is necessary to have precise prediction to maintain system stability. This makes MSE a fitting metric of assessing model effectiveness in predicting the dynamic behavior of the two-wheeled wheelchair system.

Initially, the model structure in the hidden layer was set to 2 neurons. A summary of performance for the system identification process is shown in Tables 5 and 6.

It is noted in Table 5 that as the number of delays increased to up to 7, the *MSE* decreased and for delay signal settings greater than 7 there was an increasing trend in the value of *MSE*. Therefore, it can be concluded that using the input and output signals of 7 delays, the excellent one-step-ahead prediction is acquired.

No. of delay	Epoch	MSE
1	7	0.0187010
2	20	0.0096261
3	8	0.0060088
4	25	0.0056483
5	13	0.0056063
6	24	0.0056555
7	29	0.0055486
8	20	0.0058361
9	35	0.0056977
10	18	0.0058016

Table 5. Performance of ANN with different number of delay signals.

Table 6. Performance of NN with different number of hidden neurons.

Hidden neurons	Epoch	MSE
2	16	0.0058760
4	8	0.0056716
6	7	0.0054263
8	99	0.0044463
10	7	0.0057000
12	7	0.0053779
14	15	0.0056429
16	19	0.0058035
18	7	0.0050014
20	9	0.0048871



Figure 5. NARX neural network with 8 neurons in the hidden layer and 7 delay signals.

The NN performance was then evaluated with different number of neurons in the hidden layer. Table 6 displays the results of the system prediction as the number of neurons in the hidden layer was varied. It is noted that the best MSE value was achieved with 8 neurons in the hidden layer. Hence, given both the configuration of the model and the number of delays, the best results are obtained with a combination of 7 input-output delays and 8 neurons in the hidden layer. The model with this structure was used in further evaluations.

Figure 5 shows the NN structure thus devised and used in the research. The network architecture consists of input layers that take past inputs (motor speed data) and past outputs (angular position), hidden layer with eight number of neurons that apply non-linear activation functions, an output layer that predicts the current output (angular position).

The controllers were optimized by manipulating the scaling factors and simulated in MATLAB Simulink. The performance indices for both controllers were different, as shown below, due to the different control efforts from the controllers.

A configuration with 50 iterations and 100 number of particles was used to obtain the scaling factor for both controllers. The cost function decreased as the iteration increased because the new *gbest* values tended to produce smaller errors. Hence, the cost function became smaller. As is evident in the convergence graphs in Figure 6, the PSO algorithm converged after 15th iteration and settled at 50th iteration.

For PD-type FLC, Table 7 shows the scaling factors with the minimum cost for each performance index. Moreover, Figure 6 shows the convergence of PSO, leading to the minimum cost value.

Similarly, for PID-type FLC, Table 8 shows the scaling factors with the minimum cost for each performance index. Moreover, Figure 7 shows the convergence of PSO leading to the minimum cost value.

Figures 8 and 9 show the performance of the developed system with PD-type and PID-type controllers, respectively. For FLC optimization with PD-type controller as seen in Figure 8, four sets of scaling factors optimized from ISE, IAE, ITAE, and MSE could stabilize the two-wheeled wheelchair in the upright position. Table 9 tabulates the general responses data for all the criteria. As can be observed, even after optimization with the four criteria, none of them had the ability to reduce the steady-state error to zero. The average settling time for the four sets of scaling factors was approximately 40 s and the overshoots slightly over 0.8 deg. The controller optimized with IAE criterion performed the best in terms of settling time for 38 s.

FLC optimization with PID-type controller illustrated as in Figure 9 while Table 10 is the general response data of each criterion. Only three sets of scaling factor optimized from ISE, IAE, ITAE, and MSE were able to stabilize the two-wheeled wheelchair in the upright position. Scaling factors obtained with the ISE performance index could not stabilize the wheelchair at all. The other three sets had a similar performance in terms of steady-state error. IAE and ITAE optimized controllers had higher overshot with over 0.8° compared to the others but shorter settling time of around 25 s. The system with MSE optimized controller had around 35 s settling time which ranks after IAE and ITAE.

Thus, a two-wheeled inverted pendulum has been successfully developed and controlled with an optimized fuzzy logic controller. As discussed above, although the PD-type FLC was able to stabilize the system in closed-loop form, it could not maintain the 0° tilt angle; it had a slight steady-state error even with four optimization criteria. PID-type FLC was superior to its PD-type counterpart in terms of settling time and steady-state error, MSE optimization as the best



(c) ITAE performance

(d) MSE performance

Figure 6. Performance for PD-type FLC (a) ISE performance. (b) IAE performance. (c) ITAE performance. (d) MSE performance.

Table 7. S	Scaling	factor	after	optimized	for	PD-type	FLC.
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	KI	К2	К3	Cost
IAE	-0.5199	0.1064	543.5539	11.2193
ISE	-0.455	0.0705	732.7038	5.7620
ITAE	-0.3923	0.0754	697.7447	29.6029
MSE	-0.4836	0.0846	657.3913	8.4849

Table 8.	Scaling factor	after optimized	d for	PID-type	FLC.

	KI	К2	К3	К4	Cost
IAE	0.3610	-0.1257	782.5189	-43.8427	8.7604
ISE	0.6541	0.4246	813.4782	314.0225	5.65
ITAE	0.3466	-0.1254	789.5302	-46.1152	12.5139
MSE	0.4366	-0.1033	828.8217	-32.4057	6.5937



(c) ITAE performance

(d) MSE performance

Figure 7. Performance for PID-type FLC (a) ISE performance. (b) IAE performance. (c) ITAE performance. (d) MSE performance.



Figure 8. System response with optimized PD-type FLC.



Figure 9. System response optimized PID-type FLC.

Table 9. Tabulated response with optimized PD-type FLC.

	Settling time (s)	Overshoot (°)	Steady-state error (%)
IAE	38	0.87	10
ISE	42	0.85	10
ITAE	40	0.86	10
MSE	40	0.81	10

Table 10. Tabulated response with optimized PID-type FLC.

Settling time (s)	Overshoot (°)	Steady-state error (%)
25	0.86	0.034
inf	0.80	Inf
25	0.85	0.025
35	0.81	0.046
	Settling time (s) 25 inf 25 35	Settling time (s) Overshoot (°) 25 0.86 inf 0.80 25 0.85 35 0.81

overall which allocate improvement at 12.5% of settling time and achieved negligible steady-state error at an average of 0.046%.

Conclusions

A control approach based on fuzzy logic for stabilization of a two-wheeled wheelchair to aid people with disabilities has been presented. The system has been modeled using ANN and both PD-type FLC and PID-type FLC have been considered in the investigation. The controllers have been designed and optimized using PSO and the developed controllers have been tested and evaluated using different performance evaluation criteria pertaining to the stabilization error. It has been shown that the control system thus developed is able to stabilize the wheelchair at an upright position and the FLC optimized with

PSO makes the system performance superior. It has been further shown that the system with PID -type FLC with MSE optimization performs better that manage to attain of 35 s of settling time and a satisfying steady-state error at 0.046% than what PD-type FLC able to achieve which can be defined a 12.5% improvement in settling time and maintain a 0 degree of tilt angle. Moreover, these performances will determine the user's comfort and contribute to safety aspect as the crucial element for a two-wheeled wheelchair system.

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ORCID iD

NM Abdul Ghani D https://orcid.org/0000-0001-5568-4663

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